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3 **Changes in canal width and angle in curved canals in the resin**  
4 **blocks: pro taper next versus one shape instruments**

5  
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9  
10 **Abstract**

11 **Objective:** To compare the effect of OneShape and ProTaper Next file on the  
12 change in canal width and angle of curvature in simulated curved canal in resin  
13 blocks.

14 **Methods:** The quasi-experimental study was conducted at the Aga Khan  
15 University, Karachi, from January to March 2018, and comprised endodontic  
16 resin blocks that had inbuilt curved canals. These were randomly divided into 2  
17 equal groups and were subsequently prepared using OneShape in group A, and  
18 ProTaper Next rotary instrument in group B followed by staining with red and  
19 blue ink for comparison of pre- and post-operative images of canals. Standardised  
20 photographs were taken along with reference measuring scale. SPSS 22 was used  
21 for data analysis.

22 **Results:** Of the 60 blocks, 30(50%) were in each of the two groups. The mean  
23 pre-instrumentation angle of curvature was  $32.3 \pm 2.13$  and  $31.0 \pm 3.28$  degrees for  
24 groups A and B. The mean degree of canal straightening post-intervention was  
25  $1.5 \pm 0.5$  and  $3.6 \pm 1.38$  degrees in groups A and B ( $p < 0.001$ ). In terms of canal  
26 width changes, OneShape file removed more resin material from the canal walls  
27 compared to the ProTaper Next system ( $p < 0.001$ ).

28 **Conclusion:** ProTaper Next file significantly altered the angle of curvature in the  
29 resin block compared to OneShape file, but the amount of material removed from  
30 the canal space was significantly higher with the OneShape file compared to  
31 ProTaper Next.

32 **Key Words:** ProTaper Next, OneShape, Nickel-titanium.

33

### 34 **Introduction**

35 The introduction of Nickel-titanium (NiTi) alloys in the late 1980s led to a  
36 revolution in endodontics.<sup>1</sup> Since then various technologic advancements have  
37 been made to minimise the procedural errors, and provide effective and  
38 predictable endodontic treatment.<sup>2-4</sup> These include the incorporation of M-Wire,  
39 R-phase and controlled memory wire technology to optimise the substructure of  
40 NiTi alloys.<sup>5-7</sup> Furthermore, different cross-sectional designs and new  
41 manufacturing processes have been employed to reduce the cyclic fatigue and  
42 torsional stresses.<sup>8-10</sup>

43 The fifth generation files, including OneShape (OS), ProTaper Next (PTN) rotary  
44 files etc., came into market as a result of these modifications.<sup>3</sup> The OS file,  
45 introduced by Micro-Mega (Besoncon, France), is one of the prominent single  
46 file NiTi instruments that work in continuous rotation for endodontic  
47 preparations. This unique file system is made up of conventional NiTi alloy  
48 comprising single file with 0.25mm tip diameter and 6% constant taper. OS  
49 instrument is characterised by a variable cross-section along the blade with  
50 triangular cross-section at the tip and double S-shaped throughout the shaft.<sup>11</sup> This  
51 asymmetrical design is speculated to eliminate threading and binding of the  
52 instrument in continuous rotation.<sup>12</sup>

53 PTN is the successor to the ProTaper Universal system. These files are the  
54 combination of three significant design features that includes M-Wire  
55 technology, offset and rectangular cross-section design.<sup>13</sup> This off-centre design  
56 generates a travelling mechanical wave of motion along the active portion of a

57 file. This swaggering effect serves to reduce the engagement between dentine and  
58 file as opposed to one with centred mass of rotation. This reduction of  
59 engagement also limits any undesirable screw effect, taper lock and torque on any  
60 file. An off-centred file design also limits the probability of laterally compacting  
61 the debris and blocking the root canal system anatomy.<sup>14</sup>

62 These newly incorporated features in both OS and PTN files were claimed to  
63 provide safety during preparation of canals with adequate removal of tooth  
64 structure. Investigation of the shaping abilities of both these new NiTi files is  
65 necessary to understand the behaviour of these files. The current study was  
66 planned to evaluate and compare the effect of OSA and PTN files on the canal  
67 width changes and angle of curvature on simulated curved canal in resin blocks.  
68 The null hypothesis for the study was that there would be no difference in the  
69 shaping abilities of OS and PTN rotary files.

## 71 **Materials and Methods**

72 The quasi-experimental study was conducted at the Aga Khan University,  
73 Karachi, from January to March 2018, and comprised endodontic resin blocks  
74 with inbuilt curved canal over 30 degrees. . Exemption from the institutional  
75 ethics review committee was obtained prior to data collection, and the study was  
76 conducted using the Transparent Reporting of Evaluations with Nonrandomised Designs (TREND) statement  
77 of non-randomised trials.<sup>15</sup>

78 The estimation of sample size was done using the World Health Organisation  
79 (WHO) calculator<sup>16</sup> while keeping the mean difference in angle of curvatures as  
80  $2.75 \pm 0.43$ , level of significance ( $\alpha$ ) 1% and power of study ( $1-\beta$ ) 99% in line with  
81 an earlier study<sup>17</sup>. Endodontic resin blocks made up of clear polyester resin with  
82 simulated canals having 30-35 degrees of curvature (Endo Training-Bloc,  
83 Dentsply Maillefer, Ballaigues, Switzerland) were included using non-  
84 probability consecutive sampling. Resin blocks which were damaged and/or had  
85 canal curvature  $<30$  degrees or  $>35$  degrees were excluded.

86 All preparations were made by single investigator. Resin block coding was done  
87 for identification purposes. Each block had simulated canal which was negotiated  
88 and prepared till ISO #20 size K-endodontic file reached the apex when the  
89 simulated canal exits the resin block. The working length was taken as 1mm short  
90 of the apex using direct visualisation. After preparation, the canals were irrigated  
91 with water using 5ml irrigating syringe with continuous in-and-out motion. The  
92 simulated canals of the resin blocks were then filled with green Indian ink and  
93 preoperative photographs of each block with reference measuring scale was taken  
94 with Nikon D7000 digital single lens reflex (DSLR) camera. For standardisation, all  
95 images were taken at the same distance from the resin block.

96 The blocks were then randomly divided into two equal groups. The blocks were  
97 numbered from 1-60; all even-numbered blocks were assigned to the OS group  
98 A, while all the odd-numbered blocks were allocated to the PTN group B. Both  
99 the OS and PTN rotary instruments were used as per the manufacturers'  
100 instructions. Ethylene diamine tetra acetic acid (EDTA) foam (RC-Prep) was  
101 used as a lubricant during instrumentation. After using each instrument, the canals  
102 were flushed with 5ml water using a plastic 27-gauge irrigating tip. PTN group  
103 was prepared till X2 (25/06 file) at the working length.

104 Standardised pre- and post-operative photographs, with the reference measuring  
105 scale, were then transferred to the Adobe Photoshop 7.0. Each image was then  
106 evaluated for angle of curvature, using Schneider's method<sup>18</sup> Twelve readings in  
107 millimetres on both outer and inner walls of each block were made (Figures 1-2).

108 All assessments on the imaging software were carried out by a single assessor  
109 who was not involved in the canal preparation and was unaware of the group  
110 allocation of the resin blocks. Of the total, 12(20%) blocks were re-evaluated by  
111 the same assessor for intra-examiner reliability which turned out to be 93%.

112 SPSS 22 was used for data analysis. Independent sample t-test was used to  
113 compare the angle of curvature and canal width changes after using OS or PTN

114 rotary files. Paired sample t-test was used to compare pre- and post-  
115 instrumentation changes in the blocks. The level of significance was set at  $p < 0.01$ .

116

### 117 **Results**

118 Of the 60 blocks, 30(50%) were in each of the two groups. The mean pre-  
119 instrumentation angle of curvature was  $32.3 \pm 2.13$  and  $31.0 \pm 3.28$  degrees for  
120 groups A and B. There was a statistically significant difference between the mean  
121 degrees of straightening in both the groups, with PTN causing more straightening  
122 of the canal compared to OS (Table 1).

123 Also, there was statistically significant differences between the groups at each  
124 interval of 1mm on both the inner and outer walls from 1 to 12mm, and more  
125 canal material was removed from the outer wall compared to the inner wall of  
126 the block, with OS removing more material compared to PTN (Tables 2-3).

127

### 128 **Discussion**

129 The current study rejected its null hypothesis as the results suggested that OS  
130 rotary files showed superior maintenance of the canal curvature in the resin blocks  
131 compared to the PTN files. However, PTN files were found to be more  
132 conservative in terms of removal of resin material from the canal walls.

133 The methods used for the evaluation of shaping abilities in the current study  
134 included the evaluation of angle of curvature and canal width changes for both  
135 file systems. Schneider's method for measurement of canal curvature was used in  
136 the present study for comparison of canal curvature assessment. Among the other  
137 methods used for measurement of canal curvature, Schneider's method is the  
138 most widely used method owing to its simplicity, accuracy, reliability and less  
139 chances of error.<sup>19</sup> Schneider's method not only provided simple method to  
140 evaluate root canal curvature, but also classified the curvature into canals to be  
141 straight at 5 degrees or less, moderately curved at 10-20 degrees, and severely  
142 curved at 25-70 degrees.<sup>19, 20</sup>

143 The present study used resin blocks having simulated canals with curvature  $>30$   
144 degrees, therefore, they can be characterised as canals with severe curvature.<sup>20</sup>

145 The results can be used to speculate the behaviour of rotary files in canals having  
146 severe curvature. The angle of curvature in the pre-operative resin blocks were  
147 similar for both the groups, therefore the selection bias is eliminated due to  
148 homogeneity in the sample population.

149 In the current study, PTN files caused significantly more straightening of severely  
150 curved canal. Caper et al.<sup>21</sup> compared various NiTi rotary systems, including OS  
151 and PTN files, and provided a contrasting result, with OS files causing  
152 straightening of 4.9 degrees compared to 3.7 degrees by PTN. However, that  
153 difference was not statistically significant. Furthermore, they had taken initial  
154 curvature of 28 degrees for both files in extracted mandibular molars. They had  
155 used Cone beam computed tomography (CBCT) imaging for data collection and measured the  
156 angle of curvature using the method devised by Estrela et al.<sup>22</sup> Their study further  
157 concluded that other rotary files, including WaveOne, Twisted Adaptive and  
158 ProTaper Universal, demonstrated a similar trend of straightening of  $>3$  degrees.  
159 Celikten et al.<sup>23</sup> used CBCT for the evaluation of shaping abilities of OS and PTN  
160 files. They had taken roots with canal curvature of 24 degrees for both PTN and  
161 OS. The resultant straightening caused by these files turned out to be of 1.8 and  
162 1.9 degrees for PTN and OS respectively, and the difference was not  
163 statistically significant.

164 D'Amario et al.<sup>24</sup> evaluated the effects of various single-file systems, including  
165 OS file, on the severely curved canal  $>40$  degrees. After the use of single files,  
166 the mean change in curvature was 2.7 degrees for OS. Similar trend was followed  
167 by other file systems and that was also not statistically different. They further  
168 declared these file systems to be efficient and safe to use because despite having  
169 severely curved pre-operative canals, only few degrees of straightening was  
170 observed.

171 Yuan and Yang<sup>25</sup> compared PTN with WaveOne files, and found that PTN file  
172 caused 10.8 degrees of straightening of canal compared to 13.1 degrees by  
173 WaveOne file. Although, PTN caused less straightening of canal, the difference  
174 was not statistically significant.

175 Ferrara et al.<sup>26</sup> compared PTN with ProTaper Universal files in severely curved  
176 root canals. Although the initial canal curvature for both the groups was around  
177 21 degrees, the straightening these files caused in clinical view was 4.5 degrees  
178 for both the files which means that both files caused more straightening even in  
179 curvatures that were moderate in magnitude pre-operatively.

180 It is evident that PTN caused more straightening of canal regardless of initial  
181 canal curvature compared to OS files which showed a variable trend among  
182 different studies. However, it appears that OS instrument showed less  
183 straightening in canals with pre-operative curvature >40 degrees. This trend was  
184 also followed in the present study that clearly showed that OS, despite being made  
185 up of conventional NiTi, clearly surpassed the M-Wire technology-based PTN  
186 files.

187 Both PTN and OS systems were compared for the removal of canal material from  
188 the resin block. Both files with same apical diameter and constant taper from tip  
189 to shaft of file i.e. 0.25mm tip diameter with 6 degrees constant taper were  
190 selected in order to exclude the effect of file size on canal preparation.<sup>23</sup> However,  
191 it is evident from the preparations that OS file was significantly more aggressive  
192 in terms of removing canal material from the resin block at each interval from  
193 apical to coronal region of the canal. This is in contrast with the findings of  
194 Alrahabi et al.<sup>27</sup> who reported PTN to be more aggressive in terms of canal width  
195 changes and ultimately causing more canal transportation than with OS in  
196 extracted teeth. Dhingra et al.<sup>28</sup> compared OS with WaveOne in extracted molars  
197 using CBCT, and also concluded that OS was less aggressive in the removal of  
198 canal dentine. Despite having similar apical diameter and taper, this behaviour  
199 can be attributed to the differences in the physical properties of both these files.



200 Since PTN file prepares canal in a swaggering manner, it can be anticipated that  
201 it poses less stresses on the canal wall, and, in turn, removes less material as  
202 opposed to files that engages all the walls of the canal simultaneously which is  
203 OS file in our case.<sup>21</sup> The other possible explanation to the mentioned result can  
204 be the physical property of resin block used itself. Endodontic resin blocks have  
205 the tendency to melt when more stresses are generated on its surface. There is a  
206 possibility that because of the aggressive nature of OS file with centred  
207 preparation engaging all the walls of the canal, it posed more stress, leading to  
208 the removal of more material compared to off centred preparation by PTN.

209 Resin blocks were used in the present study because they are standardised, easy  
210 to obtain, and eliminate the use of natural teeth for experimental procedures.<sup>29</sup>  
211 Studies have shown that preparation in resin block had similar outcome to that of  
212 preparation in a natural tooth.<sup>30,31</sup> However, concerns are also present for using  
213 them as a replacement of teeth for endodontic training purposes.<sup>32</sup>

214 Since the last decade or so, the world is shifting towards single-file systems for  
215 root canal preparations with efficient cutting potential while maintaining the  
216 original canal anatomy. No file system up till now is considered perfect in terms  
217 of these requirements. The quest for the ideal file system continues. PTN, despite  
218 its disadvantages, if used judiciously, can preserve the canal anatomy better and  
219 produce good results. Further studies on extracted teeth using three-dimensional  
220 (3D) imaging are required to obtain more precise results.

221

## 222 **Conclusions**

223 There was a significant difference in the angle of canal curvature pre- and post-  
224 instrumentation in both OS and PTN files. PTN files significantly altered the  
225 angle of curvature in the resin block compared to OS files. The amount of material  
226 removed from the canal space was significantly high with OS files compared to  
227 PTN at the apical, middle and coronal parts.

228



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230 **Conflict of Interest:** None.

231 **Source of Funding:** None.

232

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329 **Table 1: Comparison of angle of curvature in resin block OneShape versus ProTaper**  
330 **Next file systems.**

|                          | <b>Pre<br/>instrumentation<br/>(degrees)<br/>Mean <math>\pm</math>SD</b> | <b>Post<br/>instrumentation<br/>(degrees)<br/>Mean <math>\pm</math>SD</b> | <b>Mean<br/>difference<br/>(degrees)<br/>Mean <math>\pm</math>SD</b> | <b><i>p-value</i></b> |
|--------------------------|--|---|--|-----------------------|
| <b>OneShape</b>          | 32.30 $\pm$ 2.13   | 33.80 $\pm$ 2.12  | 1.5 $\pm$ 0.5  | <0.001                |
| <b>ProTaper<br/>Next</b> | 31 $\pm$ 3.28  | 34.6 $\pm$ 3.3  | 3.6 $\pm$ 1.38   | <0.001                |
| <b><i>p-value</i></b>    | 0.07   | 0.27  | <0.001   |                       |

331

• *Paired sample t test (in rows italic)*

332

• Independent sample t test (in column)

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• SD= Standard deviation

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• *p-value* <0.01 is considered as significant

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338 **Table 2: Canal width changes on inner wall after using OneShape and ProTaper Next**  
339 **files.**

| <b>Distance from apex</b> | <b>OneShape<br/>Mean <math>\pm</math> S.D. mm</b> | <b>ProTaper Next<br/>Mean <math>\pm</math> S.D. mm</b> | <b><i>p-value</i></b> |
|---------------------------|---|--|-----------------------|
|---------------------------|---|--|-----------------------|

|                     |             |             |        |
|---------------------|-------------|-------------|--------|
| Inner wall at 1 mm  | 0.84 ± 0.38 | 0.42 ± 0.36 | <0.001 |
| Inner wall at 2 mm  | 0.88 ± 0.43 | 0.51 ± 0.4  | 0.001  |
| Inner wall at 3 mm  | 0.87 ± 0.41 | 0.36 ± 0.28 | <0.001 |
| Inner wall at 4 mm  | 0.94 ± 0.34 | 0.42 ± 0.29 | <0.001 |
| Inner wall at 5 mm  | 0.89 ± 0.31 | 0.54 ± 0.39 | <0.001 |
| Inner wall at 6 mm  | 0.93 ± 0.33 | 0.57 ± 0.37 | <0.001 |
| Inner wall at 7 mm  | 0.94 ± 0.33 | 0.61 ± 0.36 | 0.001  |
| Inner wall at 8 mm  | 0.92 ± 0.29 | 0.59 ± 0.38 | <0.001 |
| Inner wall at 9 mm  | 0.96 ± 0.31 | 0.57 ± 0.39 | <0.001 |
| Inner wall at 10 mm | 0.93 ± 0.32 | 0.61 ± 0.38 | 0.001  |
| Inner wall at 11 mm | 0.98 ± 0.36 | 0.61 ± 0.43 | 0.001  |
| Inner wall at 12 mm | 0.97 ± 0.32 | 0.68 ± 0.44 | 0.006  |

- 340 • n=30 each group  
 341 • Independent sample t test  
 342 • *p*-value <0.01 is significant  
 343 • SD= Standard deviation  
 344

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347 **Table 3: Canal width changes on outer canal wall after using One Shape and ProTaper**  
 348 **Next files.**

| Distance from apex | OneShape<br>Mean ± S.D. mm | ProTaper Next<br>Mean ± S.D. mm | <i>p</i> -value |
|--------------------|----------------------------|---------------------------------|-----------------|
| Outer wall at 1 mm | 1.8 ± 1.5                  | 1.01 ± 0.66                     | 0.012           |
| Outer wall at 2 mm | 1.7 ± 1.2                  | 0.98 ± 0.67                     | 0.006           |
| Outer wall at 3 mm | 1.68 ± 1.11                | 0.94 ± 0.60                     | 0.002           |
| Outer wall at 4 mm | 1.68 ± 0.93                | 0.92 ± 0.59                     | <0.001          |

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|                     |             |             |        |
|---------------------|-------------|-------------|--------|
| Outer wall at 5 mm  | 1.69 ± 0.84 | 0.99 ± 0.59 | 0.001  |
| Outer wall at 6 mm  | 1.5 ± 0.87  | 0.96 ± 0.59 | 0.005  |
| Outer wall at 7 mm  | 1.64 ± 0.79 | 1.03 ± 0.63 | 0.002  |
| Outer wall at 8 mm  | 1.66 ± 0.78 | 1.05 ± 0.63 | 0.002  |
| Outer wall at 9 mm  | 1.65 ± 0.76 | 1.10 ± 0.60 | 0.003  |
| Outer wall at 10 mm | 1.63 ± 0.77 | 1.03 ± 0.68 | 0.002  |
| Outer wall at 11 mm | 1.62 ± 0.73 | 0.99 ± 0.69 | 0.001  |
| Outer wall at 12 mm | 1.59 ± 0.72 | 0.92 ± 0.66 | <0.001 |

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- 349     • n=30 each group  
350     • Independent sample t test  
351     • *p*-value <0.01 is significant  
352     • SD= Standard deviation

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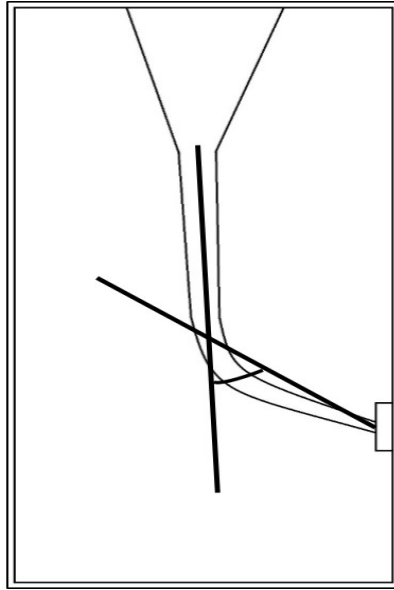
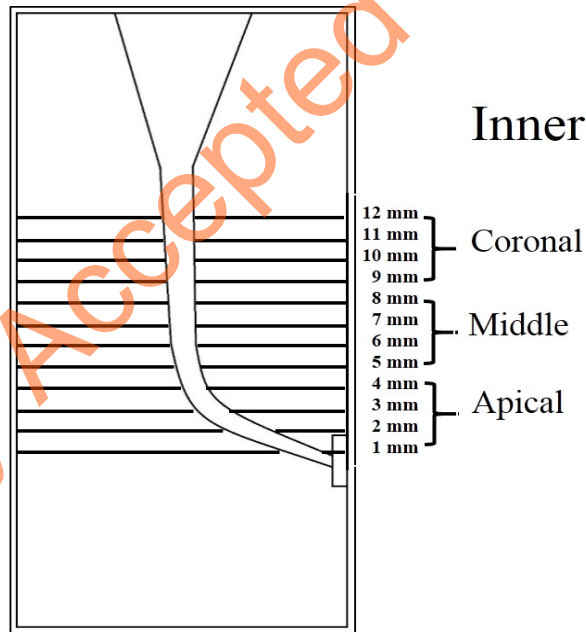


Figure 1: Measurement of angle of curvature on resin block using Schneider's method.

Outer wall

Inner wall



378  
 379  
 380  
 381

Figure 2: Description of measuring points on both inner and outer walls of resin block with simulated canal.

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